

# Interactive Voxel based Cutting of Deformable Models at Arbitrary Resolution

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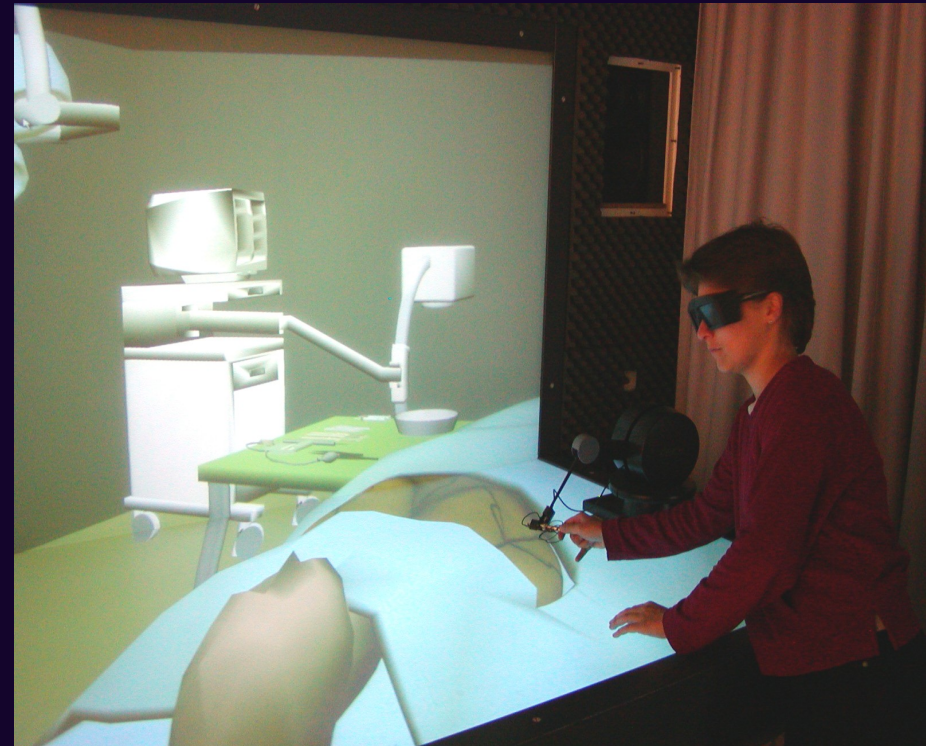
EVASION Group



# Motivation: Virtual Surgery

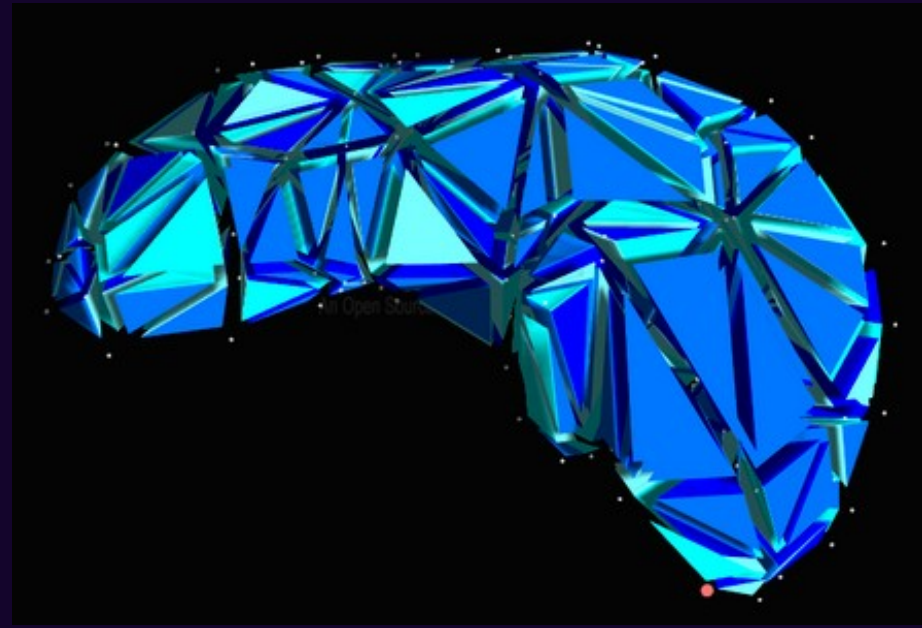
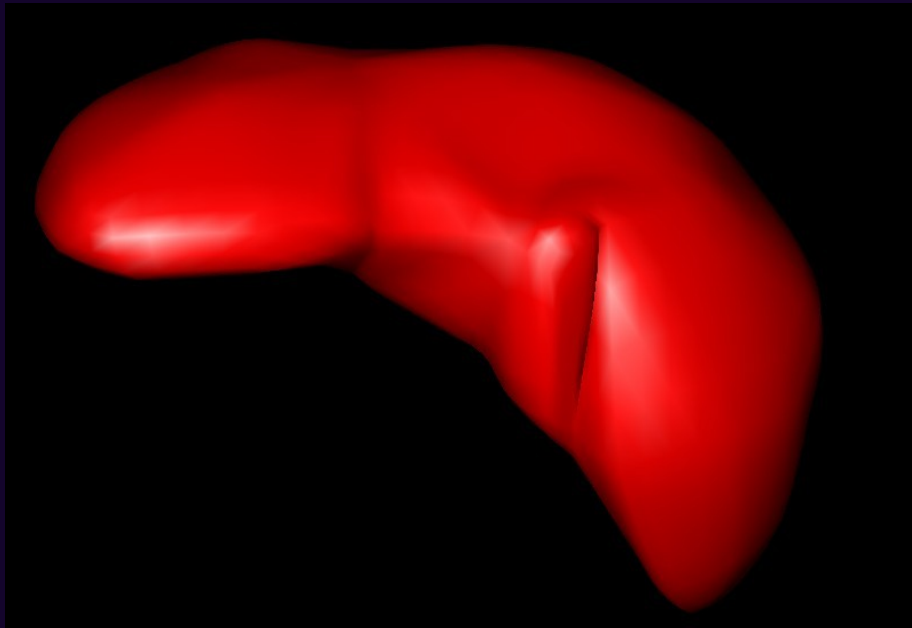
## Requirements:

- patient specific data
  - mechanical properties
  - visualization
- interactive soft tissue deformation
- **stable interactive cutting of soft tissue**
- force feedback



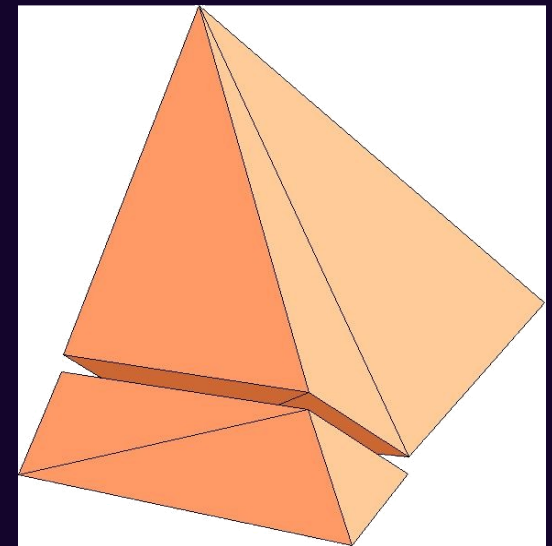
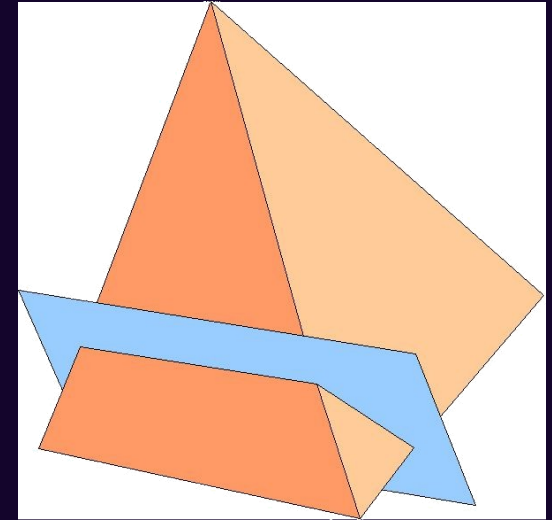
# State of the Art - Deformation

- The Finite Elements Method (FEM) approximates the object using a volumetric mesh of simple elements (e.g., tetrahedra) connected at nodes



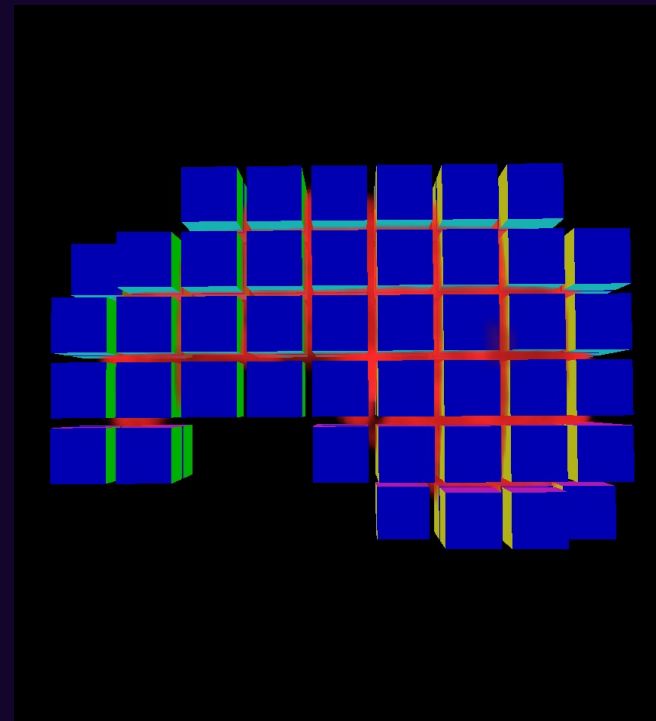
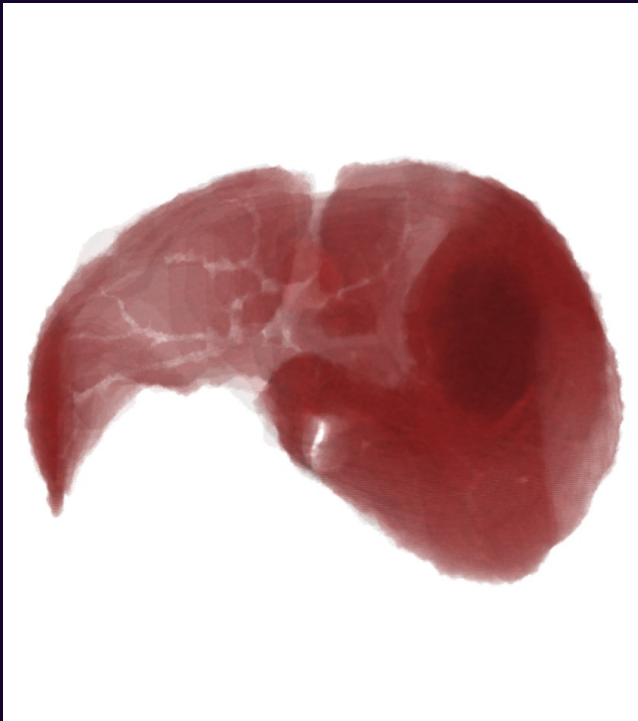
# State of the Art - Cutting

- A cut is modeled by subdividing the elements (local remeshing)
- Problems
  - Increasing number of elements
  - Simulation instability due to small and ill shaped elements



# Voxel based Approach

Interactive liver surgery using hexahedral finite elements



# Why voxels?

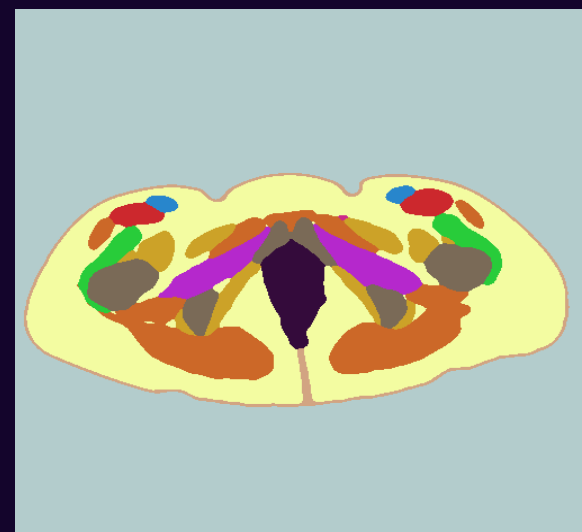
## Medical data are voxels

- no loss of information due to conversions



## Regular grid

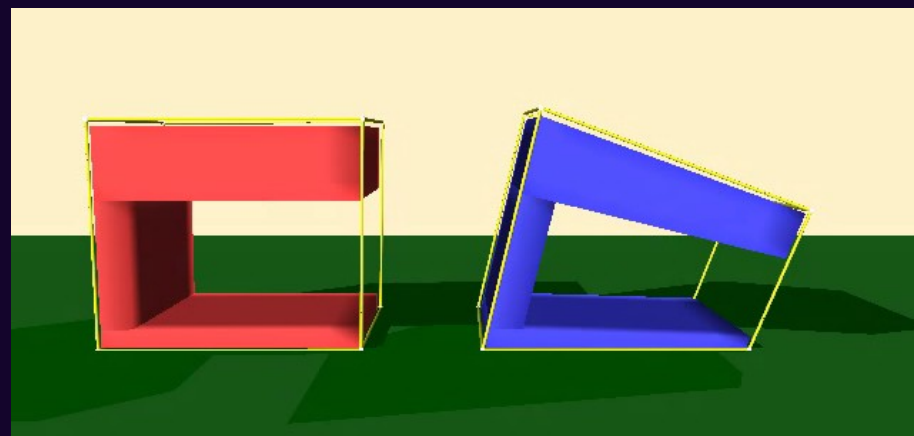
- straight forward hierarchies (octree)
- 3D texture (convenient for GPU implementations)



# Voxel based Approach - Deformation

## Nonuniform stiffness

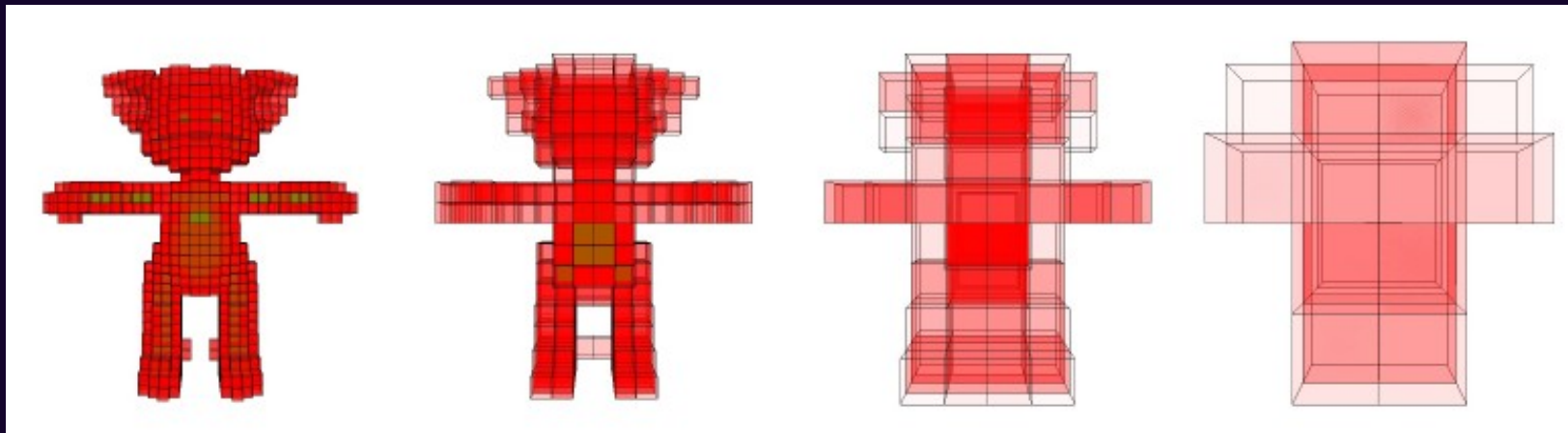
- M. Nesme et al. (2006), *Animating Shapes at Arbitrary Resolution with Non-Uniform Stiffness*. In: Eurographics Workshop in Virtual Reality Interaction and Physical Simulation (VRIPHYS'06)



# Nonuniform Stiffness

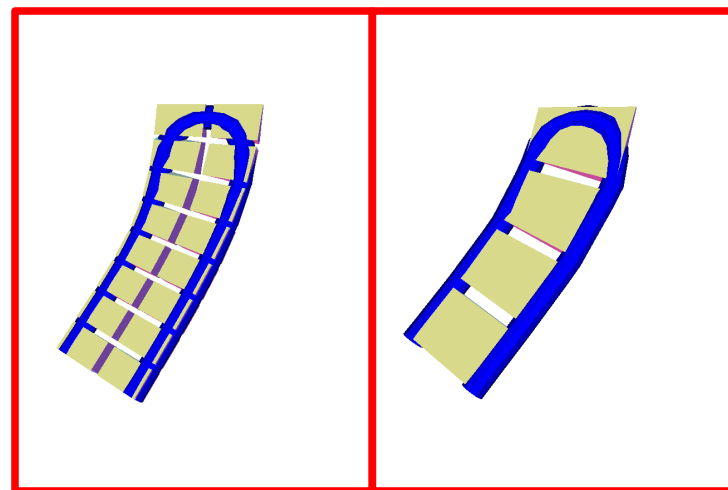
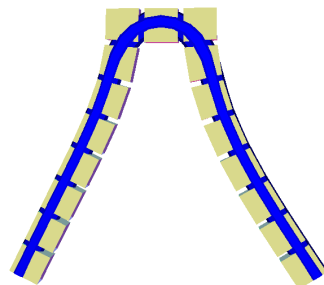
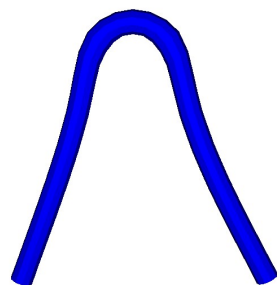
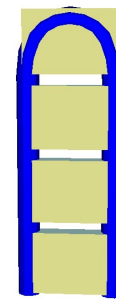
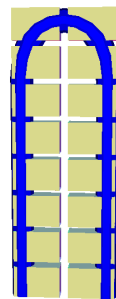
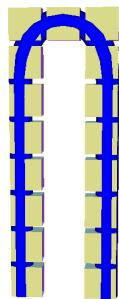
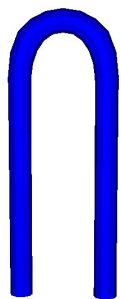
## Simulation at arbitrary resolution

- a small number of coarse finite -> efficient simulation
- preservation of fine details for visualization
- BUT: problems with branched objects

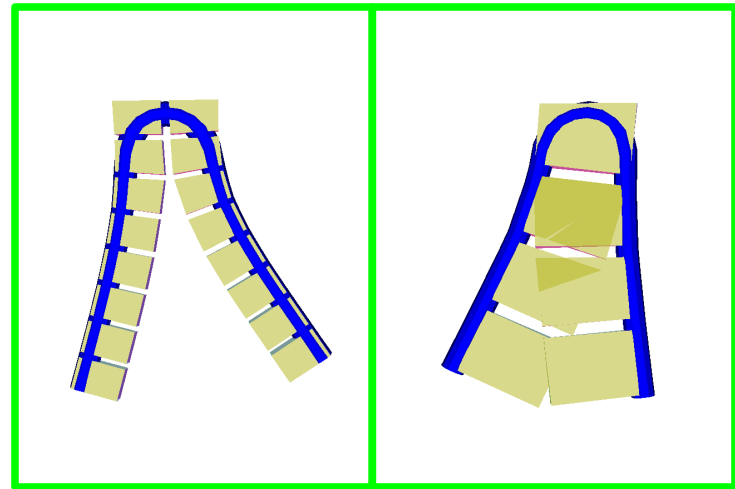
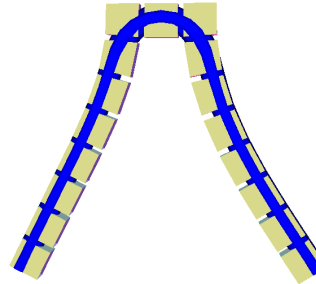
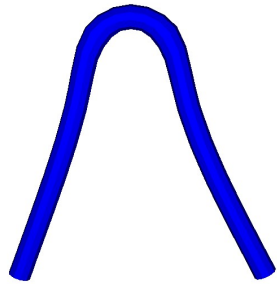
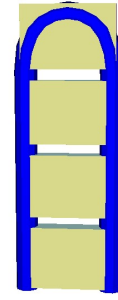
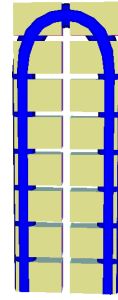
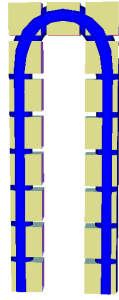
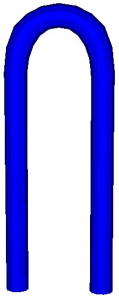




# Objects with Branches - Problem



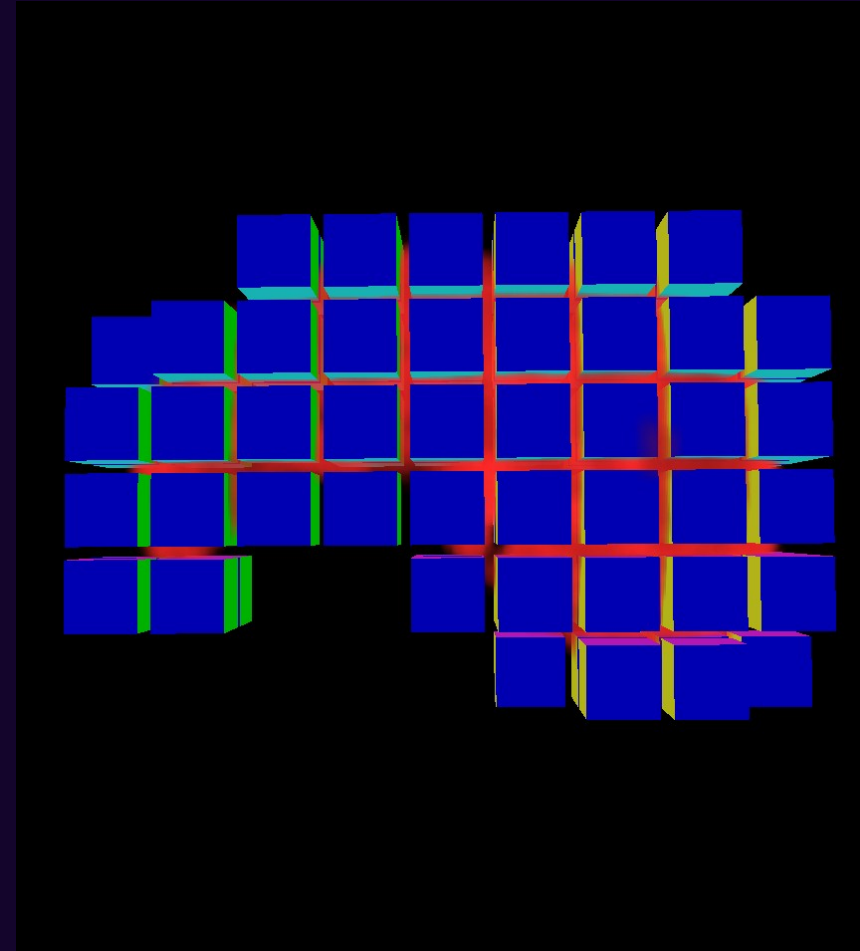
# Objects with Branches - Solution



# Cutting

Cutting = creation of branches during the simulation by removing fine voxels

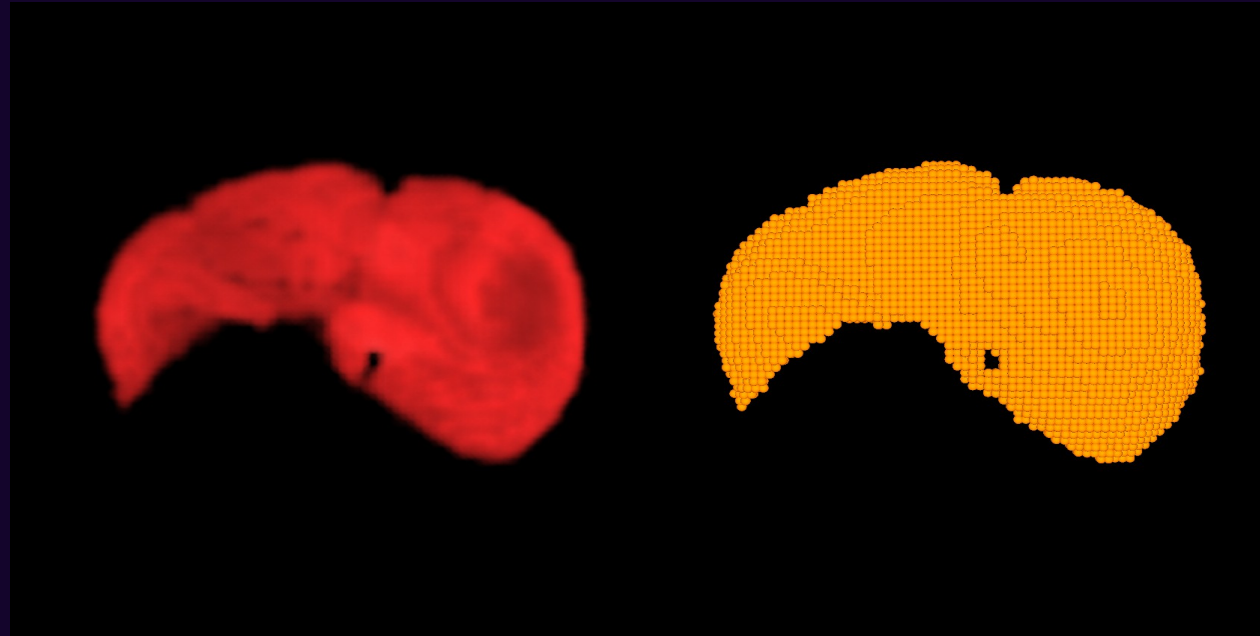
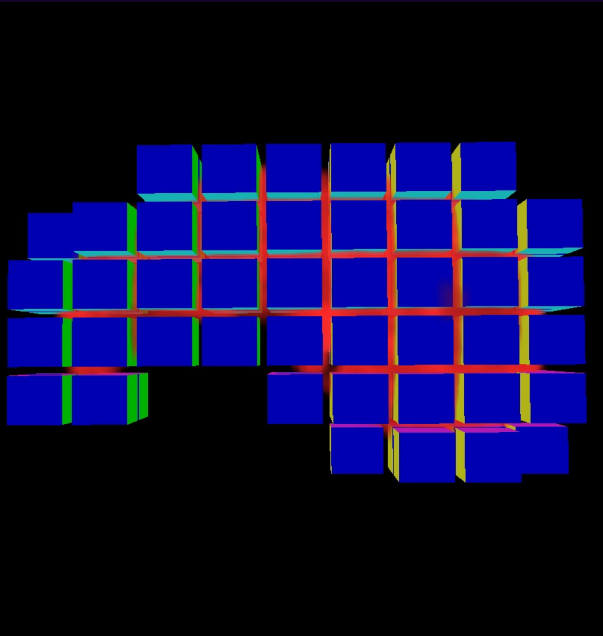
Topological changes must be propagated to all components



# Different Models for Different Tasks

coarse level

fine level



mechanical model

visual model

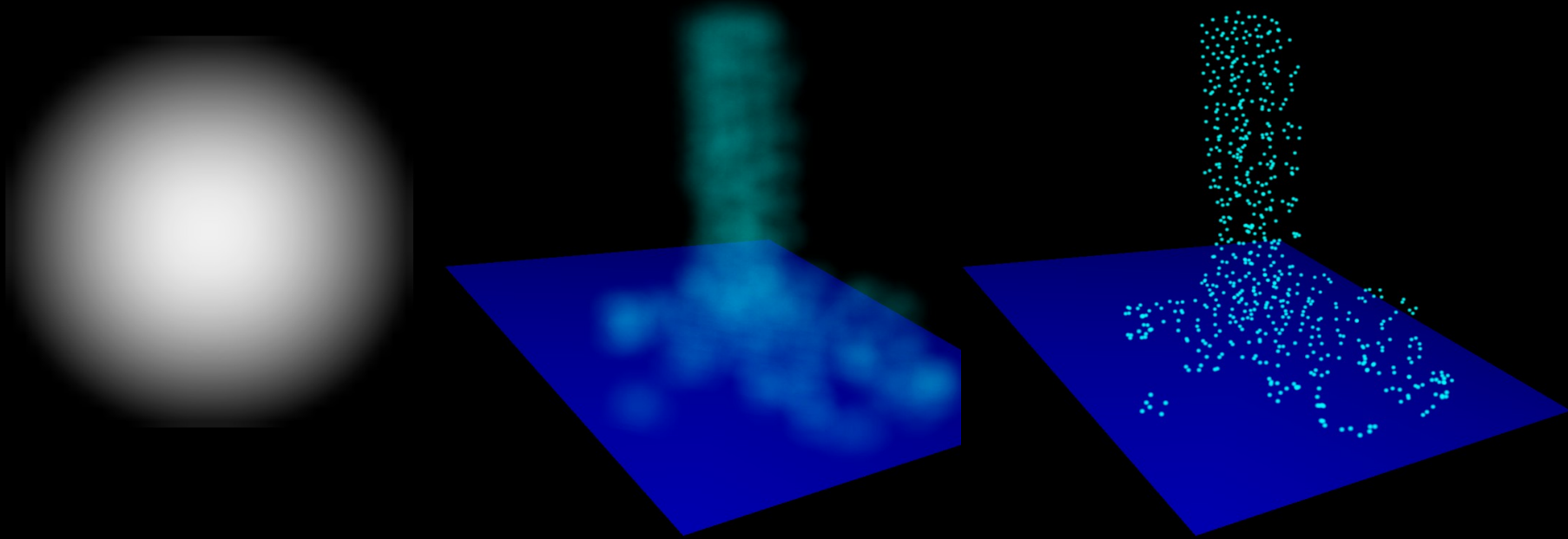
collision model



# Visual Model

## Billboarding

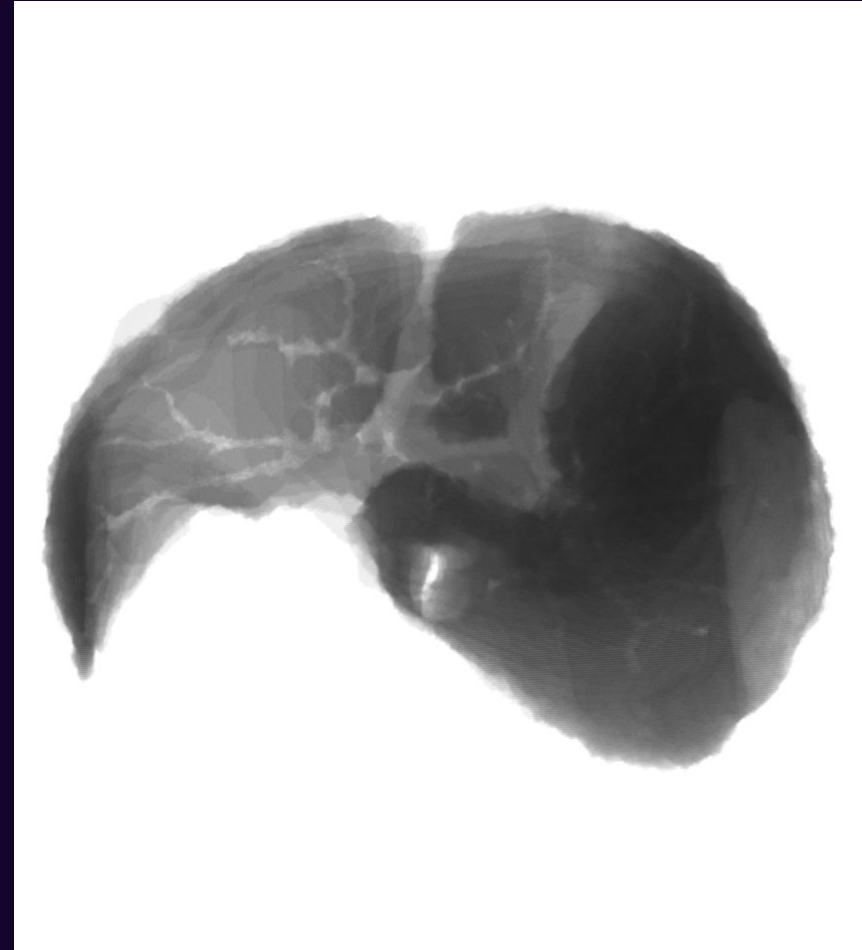
- efficient visualization of many particles
- each “sphere” consists of 1 textured quad oriented towards the camera



# Visual Model - cont.

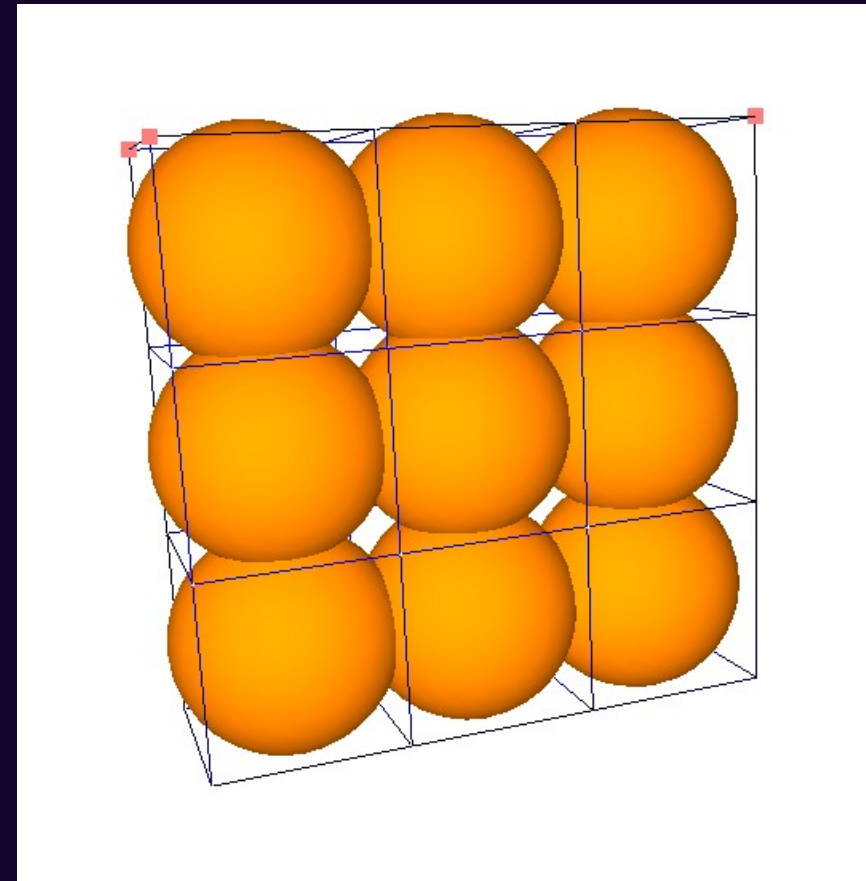
## For medical data

- use segmentation as a mask in the non-segmented dataset
- modulate color by the data



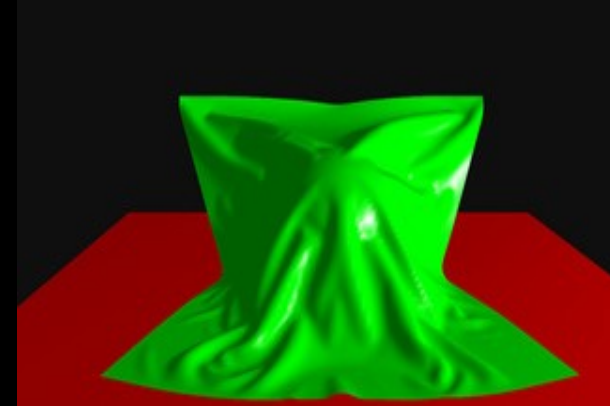
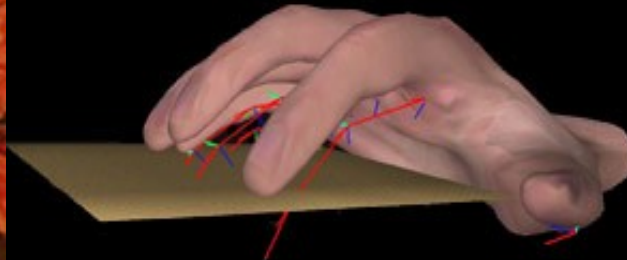
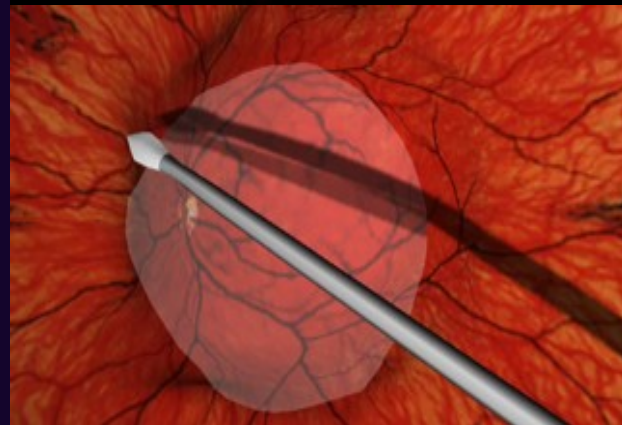
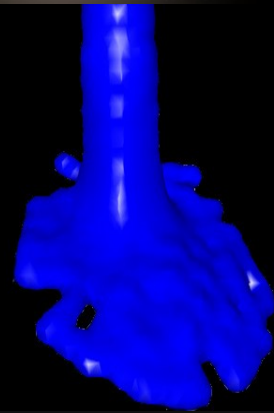
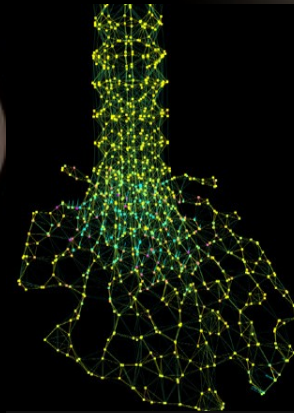
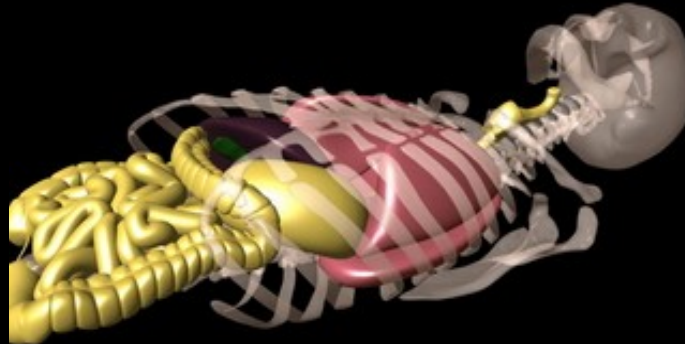
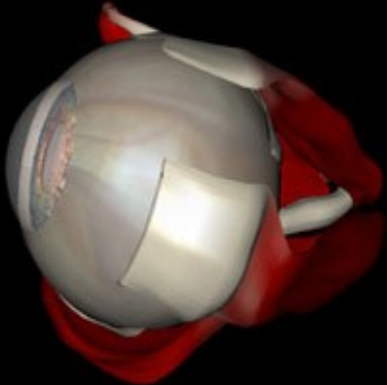
# Collision Model

A sphere in the center of each voxel



# SOFA

Simulation Open Framework Architecture



[www.sofa-framework.org](http://www.sofa-framework.org)

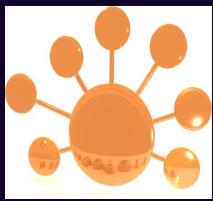


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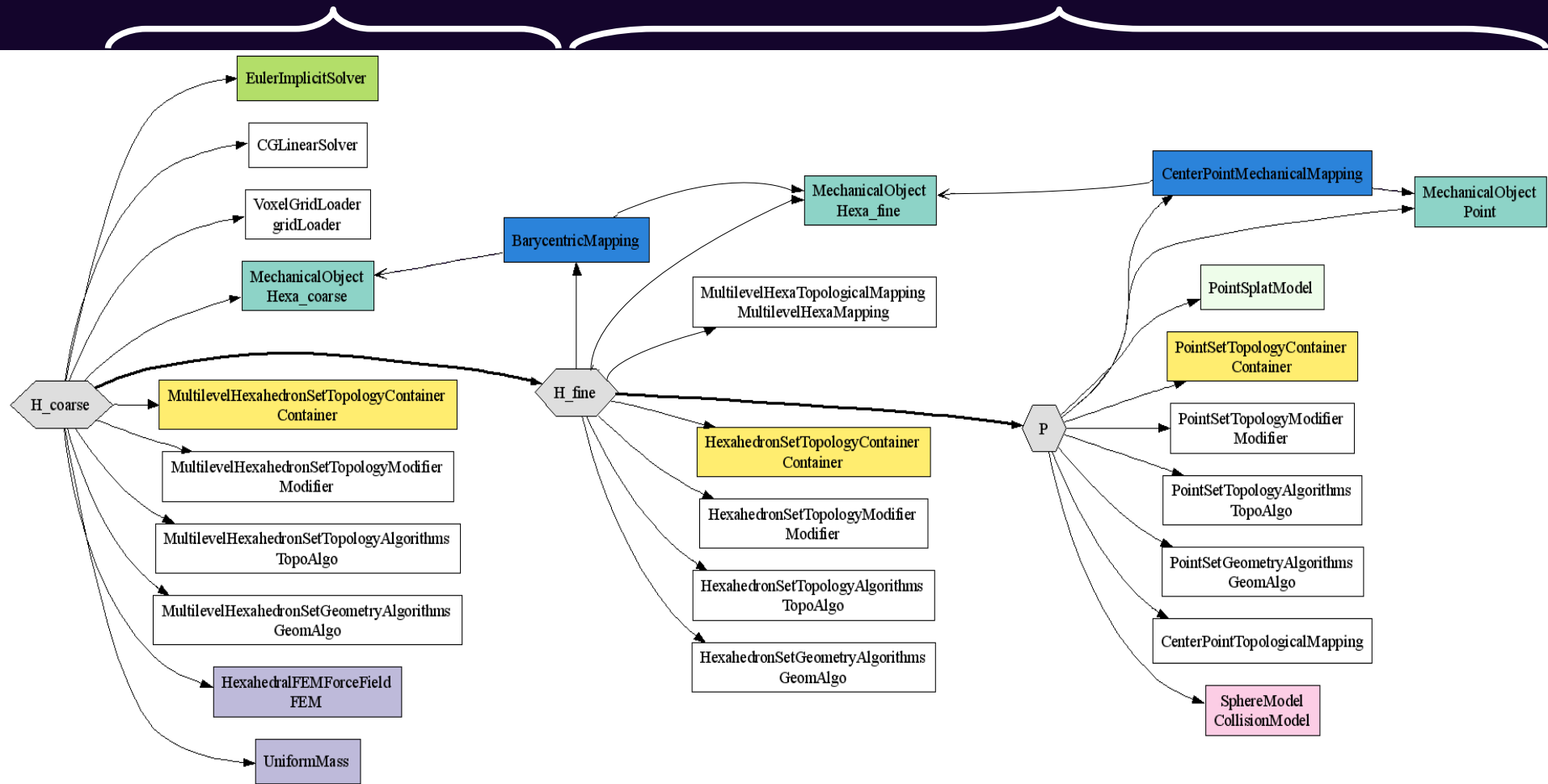




# SOFA scenegraph

coarse level

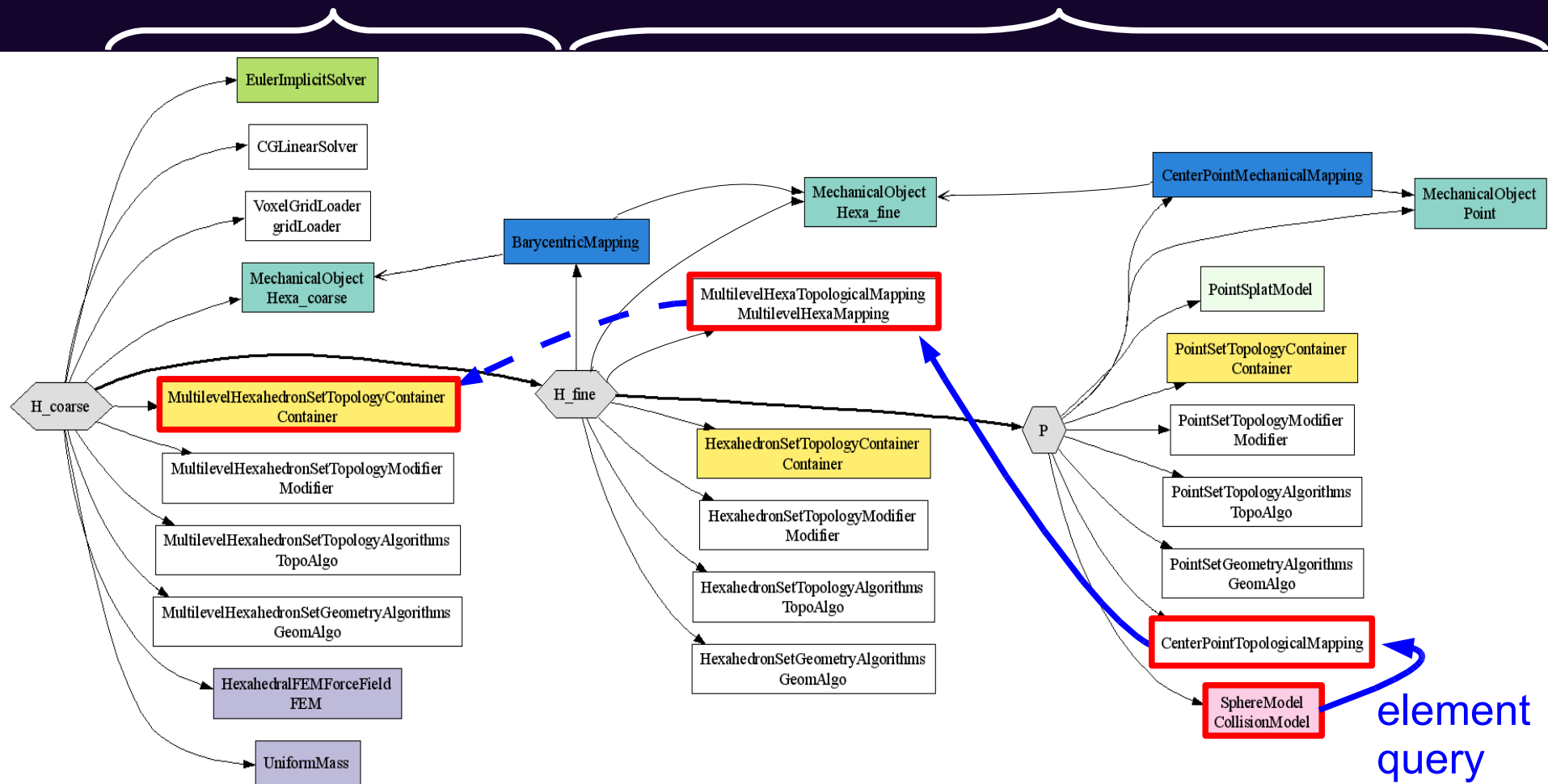
fine level



# Propagation of Topological Changes (I)

coarse level

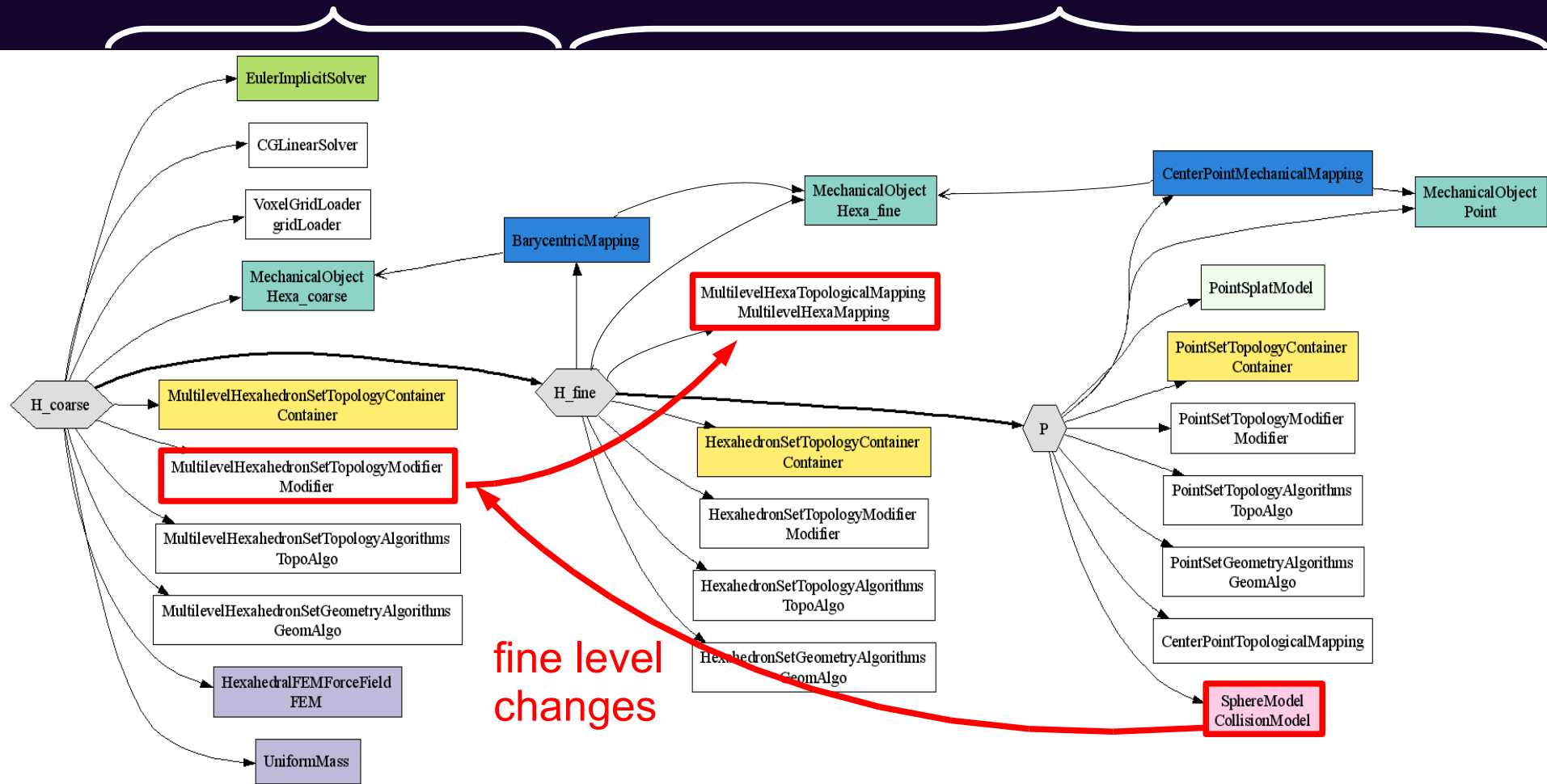
fine level



# Propagation of Topological Changes (II)

coarse level

fine level

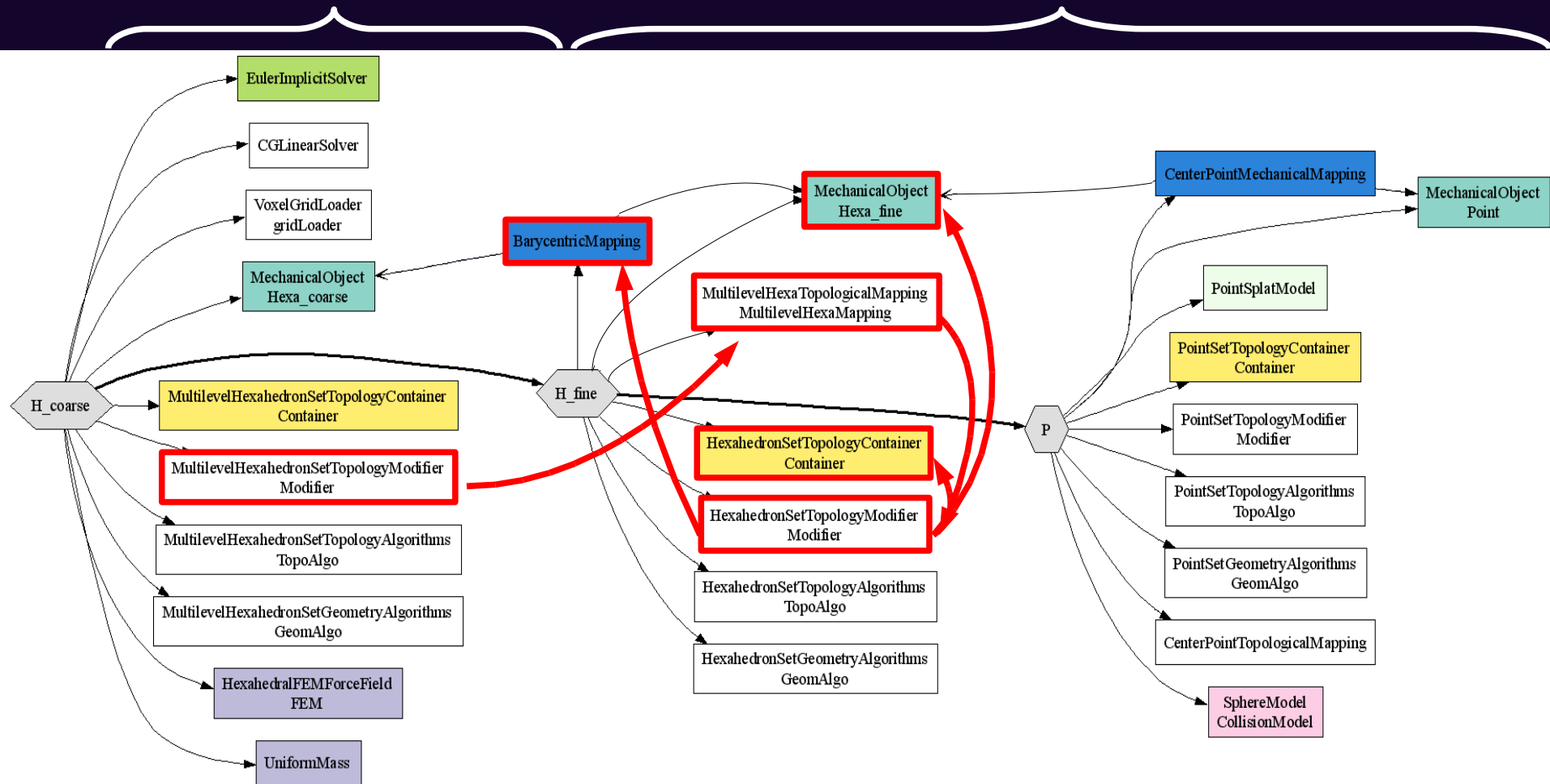


fine level  
changes

# Propagation of Topological Changes (III)

coarse level

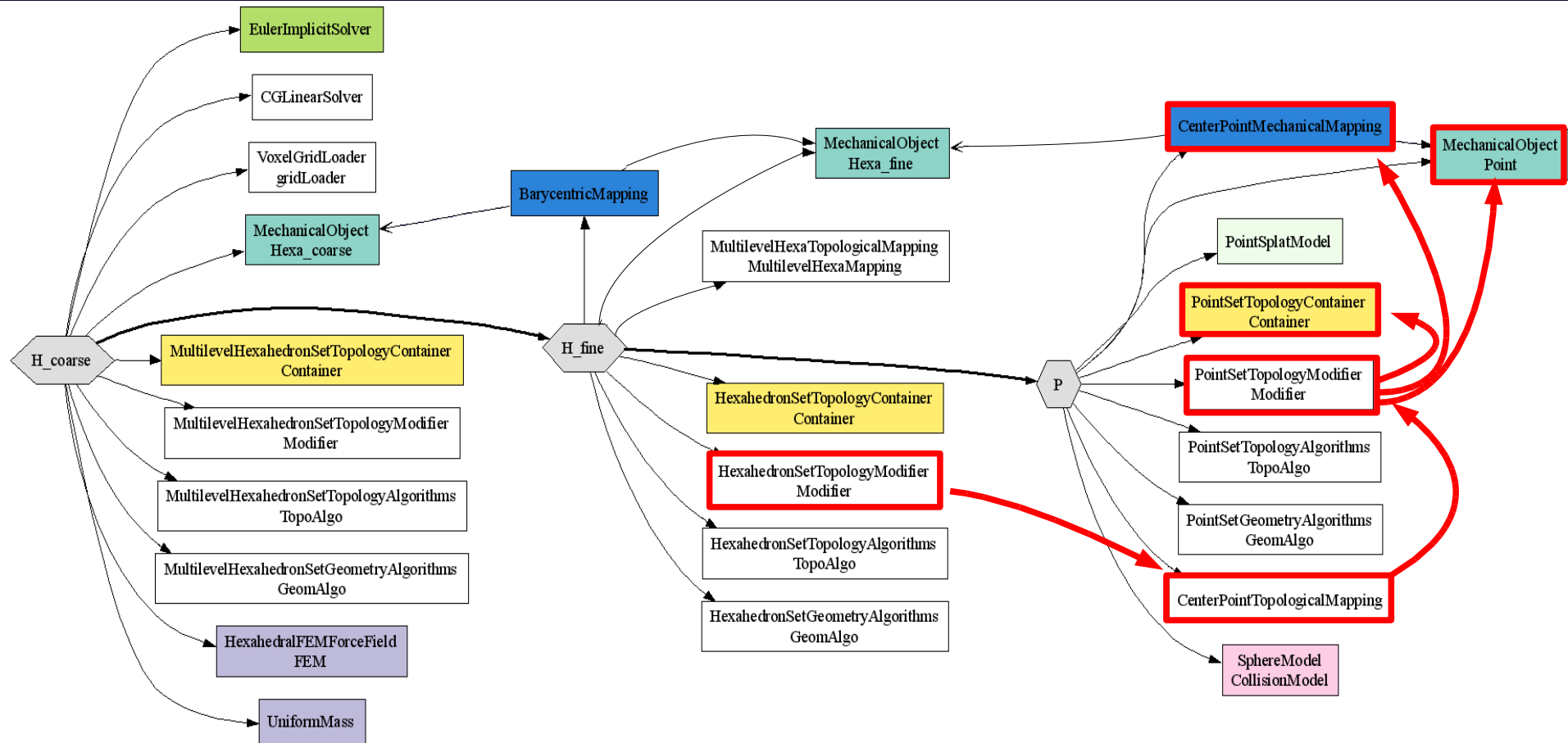
fine level



# Propagation of Topological Changes (IV)

coarse level

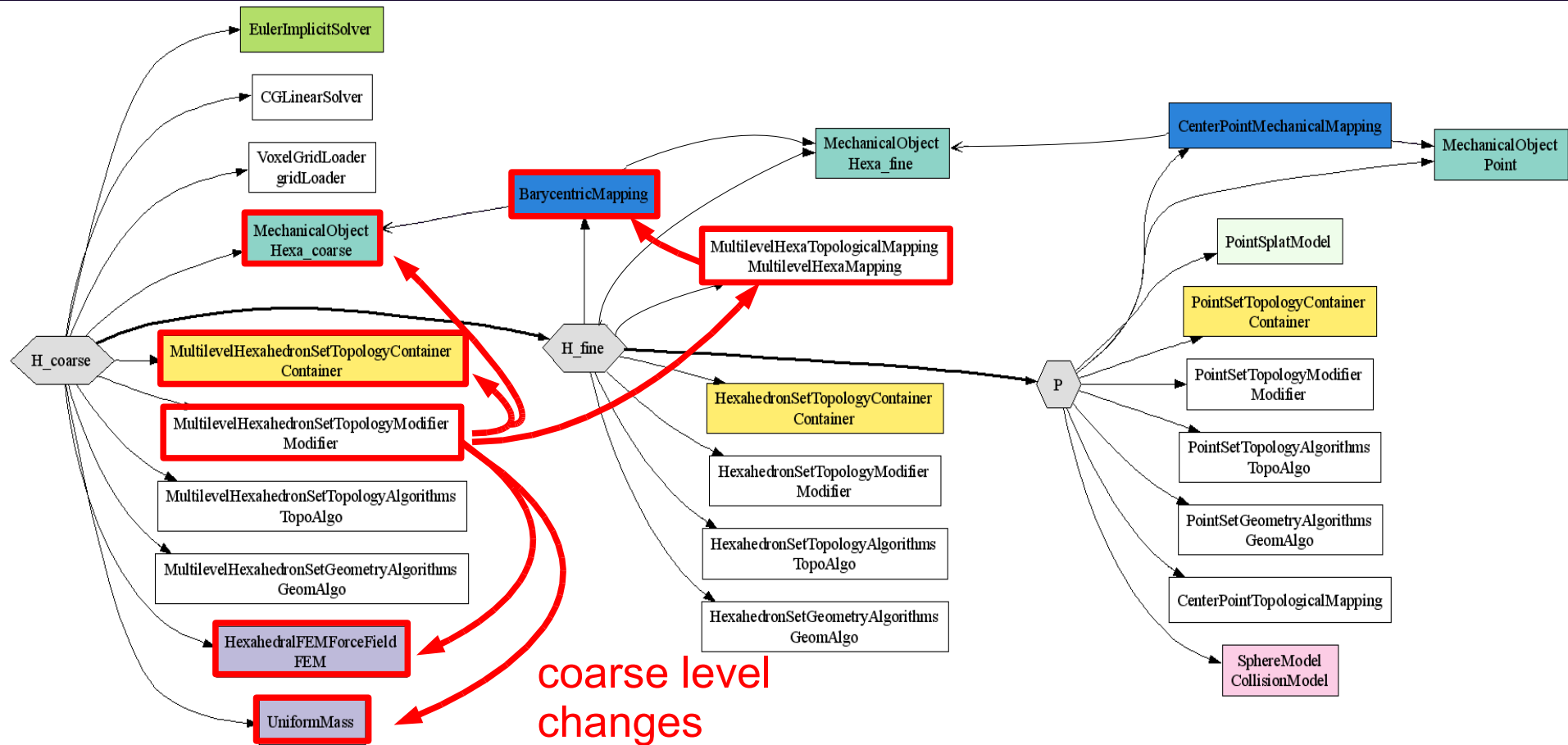
fine level



# Propagation of Topological Changes (V)

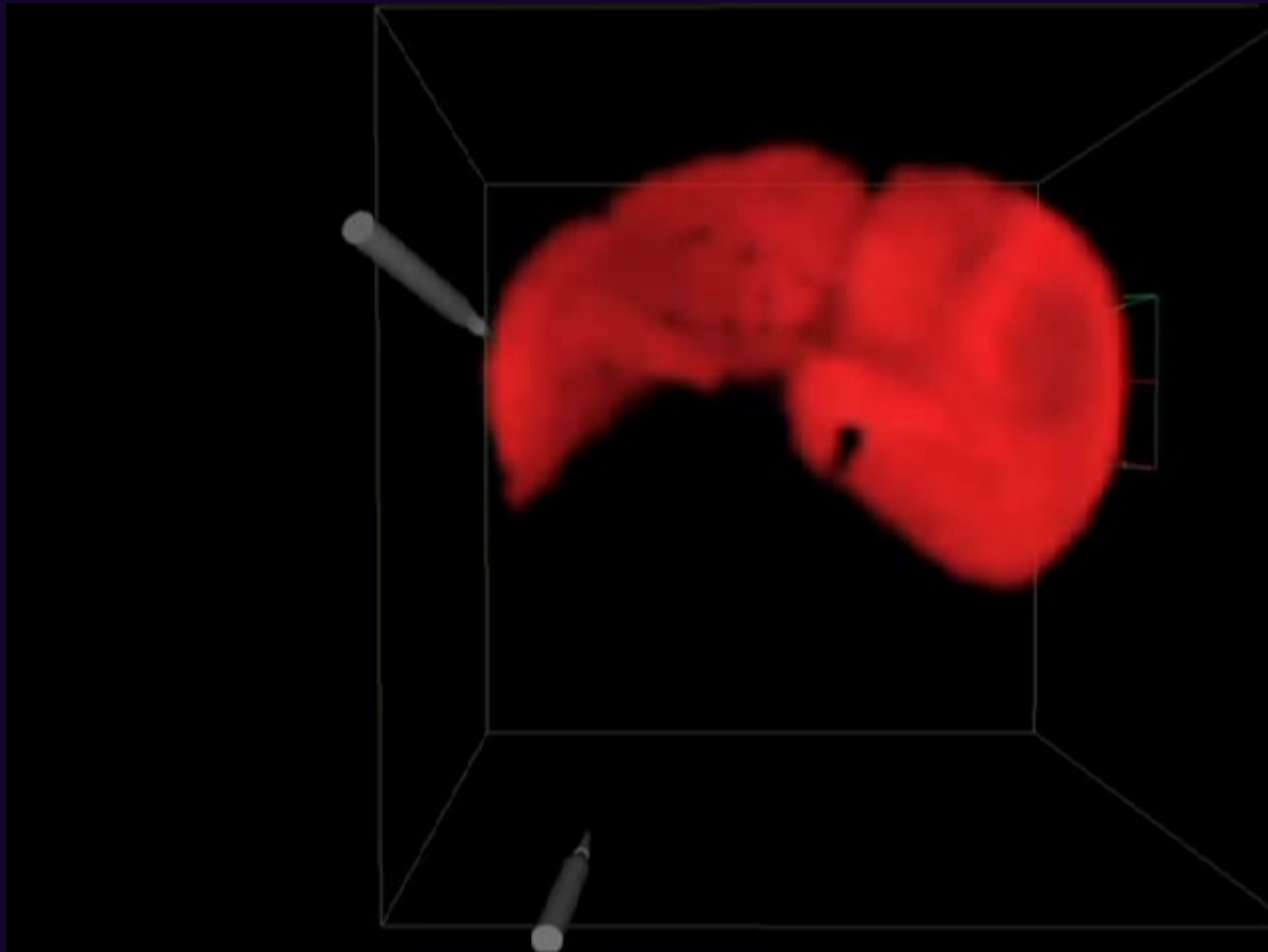
coarse level

fine level



coarse level  
changes

# Video



# Conclusion

## First prototype is working

- two level simulation
  - coarse level for physics
  - fine level for visualization and collision detection
- meshless visual and collision models
  - no connectivity problems
- efficient propagation of topological changes during the simulation
- direct use of medical data
  - patient specific simulation
- bi-manual interaction using Phantom devices

